Hypoperfusion of Brain Parenchyma is Strongly Associated with the Severity of Chronic Cerebrospinal Venous Insufficiency in Patients with Multiple Sclerosis Paolo Zamboni¹, Erica Menegatti¹, Bianca Weinstock-Guttman², Michael G. Dwyer³, Claudiu V. Schirda³,

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Background

- Chronic cerebrospinal venous insufficiency (CCSVI) is a vascular condition described in multiple sclerosis (MS) patients, characterized by stenoses of the main extracranial veins with hampered cerebral venous outflow.
- These anomalies affect the internal jugular veins (IJV), the vertebral veins (VV) and the azygous vein (AZ), and can be detected using selective venography and extracranial venous Doppler.
- Combined transcranial and extracranial echo-color Doppler (ECD) allows for non-invasive assessment of venous hemodynamic (VH) parameters indicative of CCSVI.^{1,2}
- CCSVI diagnosis requires fulfillment of at least 2 out of 5 VH abnormal criteria.
- We hypothesized that the impaired venous outflow contributes to hypoperfusion of brain parenchyma.

Objectives

• To investigate the relationship between chronic CCSVI and cerebral perfusion in patients with MS.

Methods

- Sixteen consecutive relapsing-remitting MS patients (mean age 36.1yrs, mean disease duration 7.5yrs and median EDSS 2.5) and 8 age-and sex-matched normal controls (NC) were scanned on a GE 3T scanner using dynamic susceptibility contrast-enhanced perfusion-weighted imaging (PWI) (Table 1).³
- All subjects were examined on a 3T GE Signa Excite HD 12.0 Twin Speed 8-channel scanner (General Electric, Milwaukee, WI). A multi-channel head and neck (HDNV) coil manufactured by GE was used to acquire the following sequences: 2D multi-planar dual fast spin-echo (FSE) proton density (PD) and T2-weighted image (WI); Fluid-At-Correction for patient motion prior to perfusion analysis was performed using FMRIB's Results tenuated Inversion-Recovery (FLAIR); 3D high resolution (HIRES) T1-WI using a fast Linear Image Registration Tool for Motion Correction (MCFLIRT).⁶ spoiled gradient echo (FSPGR) with magnetization-prepared inversion recovery (IR) pulse, SE T1-WI both with and without a single dose intravenous bolus of 0.1 mMol/ • Using the first steady-state volume before contrast arrival time, we applied FMRIBs and none of the NC (Table 1). Kg Gd-DTPA 5 min after injection and perfusion-weighted imaging (PWI). Scans were Linear Image Registration Tool (FLIRT) to derive an affine matrix providing a transforprescribed in an axial-oblique orientation, parallel to the subcallosal line. There was a significant association between VH criteria and VHISS, and CBF, CBV mation from the native perfusion acquisition space to the high-resolution FLAIR space. and MTT in all examined regions of the brain parenchyma in MS patients (Table 2).
- All 16 MS patients fulfilled the diagnosis of CCSVI (median VH=4, median VHISS=9) This matrix was then used to co-register perfusion MTT, CBF, and CBV maps into • PWI was acquired during and after injection of Gd-DTPA (15mL 0.1 mmol/kg) with an the subject-specific upsampled FLAIR space. These maps were then overlaid onto all • The most robust correlations were observed for lower CBF and higher VHISS in the MRI-compatible power injector at a speed of 5 ml/s. The NC were also injected with the References GM and WM (r= -0.70 to -0.72, p<0.002) (Figure), and in the thalamus, caudate, contrast agent. Single-shot gradient-echo EPI was used with the following parameters: relevant ROI masks to calculate mean values for MTT, CBF, and CBV within each tissue putamen, hippocampus and nucleus accumbens (r= -0.6 to-0.72, p<0.008). The correcompartment and each deep gray matter structure. The perfusion was measured in the TR 2275 ms, TE 45 ms, FOV 26 x 26 cm, matrix 96 x 96 (resulting in inplane voxel sizes) lation coefficients for CBV and MTT were somewhat lower. . Zamboni, P., Galeotti, R., Menegatti, E., et al. A prospective open-label study of endovascular treatment of of 2.71 x 2.71 mm), 20 slices (7 mm thick) with no gap. Forty time points were acquired GM, WM, thalamus, pulvinar nucleus of thalamus, caudate, putamen, globus pallidus, chronic cerebrospinal venous insufficiency. J Vasc Surg 2009;50:1348-58 e1-3. No relationship was observed for NC between VH and VHISS and PWI outcomes. hippocampus, amygdala, nucleus accumbens, red nucleus and substantia nigra. per slice.
- A diagnosis of CCSVI was established based on the VH Doppler criteria 2 and the Conclusion • PWI characteristics of the various regions studied, including deep gray matter structures and gray matter (GM) and white matter (WM) tissue compartments were assessed. severity was based on fulfilled the VH criteria (score 0-5) and VH insufficiency severity score (VHISS) (score 0-16).³
- rol 2009:24:133-8. • This study demonstrates that the severity of CCSVI is strongly associated with hypo-• Calculation of perfusion cerebral blood flow (CBF), blood volume (CBV) and mean 4. Dwyer, M. G., Bergsland, N., Saluste, E., et al. Application of hidden Markov random field approach for perfusion of the brain parenchyma in MS. transit time (MTT) was conducted using a previously described technique. ⁴ Briefly, we Correlation analysis (Spearman) was used to assess the relationship between PWI quantification of perfusion/diffusion mismatch in acute ischemic stroke. Neurol Res 2008;30:827-34. used the Java Image Manipulation software package (Xinapse Systems, Thorpe Wameasures and VH, VHISS. No correction for multiple comparisons was performed for Disclosure 5. Morgan, B., Utting, J. F., Higginson, A., et al. A simple, reproducible method for monitoring the treatment of terville, UK) ⁵ with an automated AIF-finding algorithm and singular value decompositumours using dynamic contrast-enhanced MR imaging. Br J Cancer 2006;94:1420-7. correlation analyses, given the exploratory nature of the study and low sample size. tion for perfusion curve fitting. CBF and CBV values were relative, based on estimated Jenkinson, M., Bannister, P., Brady, M., et al. Improved optimization for the robust and accurate linear reg-We considered p<0.05 as significant. • This study was funded by the Hilarescere Foundation and research funds at the istration and motion correction of brain images. Neuroimage 2002;17:825-41 tissue relaxivity parameters. Buffalo Neuroimaging Analysis Center and Jacobs Neurological Institute.





Table 1. Demographic, clinical, venous hemodynamic and MRI characteristics of relapsing-remitting MS patients and healthy controls.							
	Multiple Sclerosis (n-16)	Healthy Controls (n=8)	р				
Female gender, n (%)	10 (63%)	6 (75%)	NS				
Age in years, mean (SD)	36.1 (7.3)	33.1 (7.3)	NS				
Disease duration, mean (SD)	7.5 (1.9)						
Age at diagnosis, mean (SD)	35.8 (9.2)						
Expanded Disability Status Scale, mean (SD)	2.4 (0.9)						
Multiple Sclerosis Functional Composite, mean (SD)	-2.5 (0.03)	-2.5 (0.02)	NS				
Treatment in years, mean (SD)	4.3 (3.4)						
Distribution of VH criteria							
VH1	12 (75%)	0 (0%)					
VH2	14 (88%)	0 (0%)	0 (0%) <0.001				
VH3	14 (88%)	1 (13%)					
VH4	13 (81%)	0 (0%)					
VH5	8 (50%)	0 (0%)					
Number of venous hemodynamic criteria, mean (SD)	3.8 (0.23)	0.12 (0.35)	<0.001				
Venous Hemodynamic Insufficiency Severity Score, mean (SD)	8.9 (2.8)	0 (0)	<0.001				
The differences between MS patients and healthy controls were assessed using the Student's t-test, Fisher Exact test and Mann-Whitney rank sum test.							



Figure. Examples of perfusion imaging maps in 2 relapsing-remitting multiple sclerosis patients with severe (right images) and less severe (left images) venous hemodynamic insufficiency severity score (VHISS). On the left side is a 33 year old RRMS patient with VHISS 5, and on the right is a 38 year old RRMS patient with VHISS 12.





Table 2. Spearman correlation coefficients and p values between venous hemodynamic insuffi- ciency severity score (VHISS) and perfusion-weighted (PWI) measures (in bold are highlighted significant correlations) in relapsing-remitting patients.								
	Mean tra	ansit time p	Cerebral blood flow r p		Cerebral blood volume r p			
Gray matter	0.52	0.039	-0.70	0.002	-0.58	0.019		
White matter	0.53	0.034	-0.71	0.002	-0.49	0.054		
Right caudate	0.44	0.087	-0.45	0.078	-0.23	0.387		
Left caudate	0.53	0.033	-049	0.065	-0.33	0.214		
Right putamen	0.45	0.084	-0.70	0.003	-0.39	0.135		
Left putamen	0.45	0.077	-0.71	0.002	-0.39	0.140		
Right globus pallidus	0.37	0.154	-0.68	0.003	-0.31	0.251		
Left globus pallidus	0.43	0.099	-0.69	0.003	-0.13	0.627		
Right thalamus	0.46	0.074	-0.66	0.006	-0.51	0.044		
Left thalamus	0.46	0.077	-0.66	0.006	-0.61	0.012		
Right pulvinar thalamus	0.17	0.528	-0.67	0.004	-0.59	0.025		
Left pulvinar thalamus	0.55	0.027	-0.67	0.005	-0.47	0.067		
Right hippocampus	0.40	0.123	-0.59	0.015	-0.43	0.099		
Left hippocampus	0.34	0.198	-0.61	0.013	-0.49	0.053		
Right amygdala	0.05	0.856	-0.37	0.159	-0.44	0.085		
Left amygdala	0.16	0.547	-0.51	0.045	-0.41	0.123		
Right accumbens	0.48	0.059	-0.55	0.028	-0.14	0.608		
Left accumbens	0.52	0.041	-0.64	0.008	-0.27	0.305		
Right red nucleus	0.37	0.156	-0.54	0.033	-0.43	0.099		
Left red nucleus	0.32	0.234	-0.54	0.029	-0.46	0.075		
Right substantia nigra	0.13	0.627	-0.59	0.017	-0.31	0.251		
Left susbstantia nigra	0.19	0.481	-0.53	0.034	-0.16	0.565		

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